# Nuclei Detection in Skin Whole-Slide Histopathological Images

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# Abstract

Skin cancer is one of the most malignant types of cancer and melanoma is the most aggressive type among skin cancers. In melanoma diagnosis, analysis of various processes on the images in cellular and architectural levels are needed and the collection of information resulted from these processes is the basis of diagnosis of melanoma stage. Nuclei are important for both diagnosis and detecting other entities in cellular level; thus, we aimed to detect nuclei in histopathological images of skin biopsies, using an AdaBoost classifier. First, a set of features containing intensity-based and structure-based features was created. Then, we used AdaBoost to train on features and create a strong learner from a series of rules from weak learners based on pixel features. As a post-process step, morphological functions were applied to the results.

# 1 Introduction

The incidence of melanoma is rising faster than any other cancer, and 1 in 50 U.S. adults will be diagnosed with melanoma this year alone. The gold standard for diagnosis of skin cancer is the histopathological examination which the specimen is examined by pathologist manually [Cireşan et al., 2013]. However, the whole slide image of one tissue sample usually has the size of  $2.2 \times 10^9$  pixels, which impose large difficulty for the pathologist to analyze the image completely. Thus, manual diagnosis only based on a small portion of the image is often subjective and prone to variability and automated diagnosis based on the entire slide is more desired [Lu and Mandal, 2012].

In melanoma diagnosis, analysis of various processes on the images in cellular and architectural levels are needed and the collection of information resulted from these processes is the basis of diagnosis of melanoma stage. Nuclei are important for both diagnosis and detecting other entities (i.e. melanocytes, mitotic figures) in cellular level.

Many publications on nucleus detection are available. A simple and often used technique is thresholding. Other techniques contain fuzzy c-means clustering [Hafiane et al., 2008] and and adaptive thresholding [Petushi et al., 2006]. However, thresholding techniques require images with a well-defined, preferably uniform background. Due to the large variation in staining uptake within an image, this is often not possible [Gurcan et al., 2009].

Edge-based segmentation techniques, which try to connect local maxima of the gradient image, like the h-maxima transform [Wählby et al., 2004], are overly sensitive to image texture. Finally, a more sophisticated approach using edge-information is the Hough transform [Ortiz de Solorzano et al., 2001]. However, the performance of this method drops for noncircular nuclei and has a high computational complexity.

There are also approaches using Machine Learning reported by in literature. Wang et al. [Wang et al., 2006] and Vink et al. [Vink and de Haan, 2011] both used Adaboost and report better performance over support vector machine, which is the baseline method for classification task. Also, it would be possible to construct a efficient classifier with a small subset of features from a large set of potentially useful feature sets, which could provide insights into good features as well.

Based on our findings, We proposed to use Adaboost for constructing the nuclues detector in skin whole-slide histopathological images.

# 2 Dataset

We had access to 240 cases of skin biopsy images, acquired by University of Washington School of Medicine in their MPATH study (R01 CA151306). This dataset contains 5 different diagnoses: Benign, Atypia, Melanoma in-situ, Invasive melanoma stage T1a, Invasive melanoma  $\geq$  stage T1b. Figure 1. shows an example of a melanoma stage T1a case. Layers of the skin on biopsy specimens are as follow: the epidermis on top, the dermis below it, and the hypodermis below that layer. We used one large image of size about 8000x4500 pixels, labeled it and divided it to training, validation and testing crops.



Figure 1: An example of a skin biopsy image, melanoma stage T1a (left) and a zoomed sample of dermis-epidermis region (right)

# 3 Method

Nuclei are important for both diagnosis and detecting other entities in cellular level; thus, we aimed to detect nuclei in histopathological images of skin biopsies, using AdaBoost classifier with two features set. The schematic flow of our proposed system can be seen in Figure 2. First, a set of features for each pixel was calculated. In addition to that, we also calculated structure-based features for the image. Since we had a very large feature space, we ran PCA on it. Then, we splitted the data and used validation set to optimize hyperparameters. Next, the optimal Adaboost classifier was trained on features to create a strong learner from a series of rules from weak learners. Then, morphological functions was applied to the output to fill the holes and have a better result. Finally, we identified the connected components in the nucleus mask and the centroid of the identified nucleus. We'll go into details of methodology in the following subsections.

## 3.1 Feature Sets

To train a detector, AdaBoost requires a set of features. Two sets of features were calculated from the images in order to train and test the classifier, as shown in Figure 3. First set of features was intensity-based [Vink et al., 2013] and the second one was structure-based features [Li and Allinson, 2008]. For the intensity-based features, we used several window sizes of S = 3, 5, 9, 15, 19, 25. Here are the features in each set:



Figure 2: An overview of proposed method.



Figure 3: Detail view of feature extraction.

## 3.1.1 Intensity-Based Features:

This set of features was applied to a window  $W_S$  of size SxS for each pixel  $p_{i,j}$ . The set contained Sum, Dynamic Range (i.e. absolute difference between the maximum and minimum pixel values in the window), Variance, Median and Haar-like (HL) features. HL features are used for taking the contrast of background and nuclei into account. These features are two types: adjacent and nonadjacent features and are calculates as below:

Haar Like Features:

• adjacent HL:

$$HL_{W_1,W_2}(p_{i,j}) = SqSum(W_{12}, p_{i,j}) - \eta . SqSum(W_1, p_{i,j})$$

$$W_{12} = W_1 + 2 \cdot W_2$$
(1)

• nonadjacent HL:

$$HLNA_{W_1,W_2,W_3}(p_{i,j}) = SqSum(W_{123}, p_{i,j}) - SqSum(W_{12}, p_{i,j}) - \eta'.SqSum(W_1, p_{i,j})$$
(2)

$$W_{123} = W_1 + 2 \cdot (W_2 + W_3)$$

• nonadjacent HL2:

$$HLNA2_{W_{1},W_{2},W_{3},W_{4}}(p_{i,j}) = SqSum(W_{1234},p_{i,j}) - SqSum(W_{123},p_{i,j}) - \eta^{''}.SqSum(W_{12},p_{i,j}) - SqSum(W_{1},p_{i,j})$$
(3)

$$W_{1234} = W_{123} + 2 \cdot W_4$$

Where  $SqSum(W, p_{i,j})$  is the sum of a square of size WxW centered around pixel  $p_{i,j}$  and  $\eta, \eta', \eta''$  represent the normalization factors. Figure 4 might be helpful to understand the calculation of this features [Vink et al., 2013].



Figure 4: Haar-like box features The sum of pixel values of the green box is subtracted from the sum of pixel values of the red box.

#### 3.1.2 Structure-Based Features:

The features in this set were basically edge detector features. Gaussian gradient magnitude, Laplacian of Gaussian, eigenvalues of Hessian matrix and the eigenvalues of the structure tensor were included in this set.

#### 3.2 PCA

After feature extraction part, we had a very large feature set since we had to calculate these features for three channel of color (i.e. RGB) with various window sizes. Therefore, we decided to use PCA to reduce the feature space size. We set the PCA to get the feature with the condition that variance ratio would be higher than 0.99.

#### 3.3 Splitting the Data

The dataset after PCA was splitted to training, validation and testing dataset. The ratio for doing this was 70% of the whole data for training and validation together and remaining 30% for testing. Then the training and validation was splitted to 90% for training and 10% for validation. We needed validation set to optimize the hyperparameters we had in our classifier.

#### 3.4 Hyperparameter Optimization

We used AdaBoost to create a strong learner from a series of weak learners. In order have an optimal AdaBoost, we used validation data to find the hyperparameters we had, which are the number of estimaters and the learning rate of AdaBoost. We itearted over learning rate with these values: [0.1, 0.3, 0.5, 0.6, 0.65, 0.7, 0.75, 0.8, 0.9, 0.95, 1] and the number of estimaters as follows: range(10, 500, step = 20). The best parameter values found to be: number of estimaters = 30, learning rate = 1.

#### 3.5 AdaBoost Classifier

AdaBboost (short for Adaptive Boosting) is a classifier which can combine the output of other learning algorithms (weak learners) with weighted sum and output a boosted classifier. It has been addressed in literature [Wang et al., 2006] and [Casagrande, 2006] that AdaBoost is more efficient and performs significantly better that SVM. The psuedocode of Adaboost is summerized in **Algorithm 1**.

Algorithm 1 AdaBoost Algorithm

- 1. Initialize the observation weights  $w_i = 1/N, i = 2, ..., N$ .
- 2. For m = 1...M:

(a) Fit a classifier  $G_m(x)$  to the training data using weights  $w_i$ .

(b) Compute:

$$err_m = \frac{\sum_{i=1}^N w_i I(y_i \neq G_m(x_i))}{\sum_{i=1}^N w_i}.$$

(c) Compute 
$$\alpha_m = log((1 - err_m)/err_m)$$

- (d) Set  $w_i \leftarrow w_i.exp[\alpha_m I(y_i \neq G_m(x_i))], i = 1, 2, ...N.$
- (e) Output  $G(x) = sign[\sum_{m=1}^{M} \alpha_m G_m(x)]$

Since it has been proven that AdaBoost can be very useful and efficient classifier, we implemented it to detect nuclei using the aforementioned feature sets.

#### 3.6 Morphological Functions

In order to fill the holes and have a better output, we used morphological functions as a postprocessing step. First we applied an *opening* function which is the dilation of the erosion of a set A by a structuring element B. Then, a *closing* function was applied to the result of opening function. Closing is the erosion of the dilation of a set of a binary image.

With on trial and error, we found out that using a opening function of size 8x8 followed by a closing of size 2x2 generates decent outputs with high accuracy.

## 3.7 Finding Cell Centroid

The final step of our proposed method is to label the individual nuclei in the image so that we could use the number of nucleus as a feature in future diagnosis task. An schematic overview of the steps followed can be seen in Figure 5. To do this, we first label the connected components in the classified mask. Then, using a area threshold (700 pixels in results presented), we identified the large components that could contain multiple cells. Finally, we apply watershed segmentation method to separate connected nucleus and label each nuclei, as shown in Figure 2 and Figure 5.

## 4 Results

#### 4.1 Visualization

The AdaBoost was applied with different feature sets, with and without morphological functions as post-processing. We also label the nuclei according to each results. Figure 6 shows the samples of the results we got in each case.



Figure 5: Overview of schemes of Nuclei labeling.

 Original
 Image: Construction of the cons

Intensity + structure wo/ morphology

Intensity + structure w/ morphology

Figure 6: Figure. Nuclei detection results. Green color indicates the nuclei which are detected by the classifier.

#### 4.2 Evaluation

To evaluate the proposed detector, we used the standard evaluation metrics on each case. The metrics are: Precision = tp/(tp + fp) where tp is the number of true positives and fp the number of false positives; recall = tp/(tp + fn) where tp is the number of true positives and fn the number of false negatives; f1\_score is the harmonic mean of precision and recall and is formulate like this: 2.  $\frac{precision + recall}{precision + recall}$ . The metrics are gathered in Table 1.

Metrics features and morph	F1_score	Precision	Recall
Intensity features wo/ morph	89.37%	84.75%	94.52%
Intensity features w/ morph	89.32%	81.23%	99.21%
Intensity + structure wo/ morph	89.40%	84.71%	94.65%
Intensity + structure w/ morph	89.28%	81.14%	<b>99.22</b> %

Table 1. Evaluation metrics for each case.

To interpret the evaluation metrics, we should take this into account that structure-based features were basically edge detection functions. Recall has the highest value when we have both intensity-based and structure based which means we have less false negative results in the output. In this case, classifier has not missed much of the nuclei. On the other hand, Precision is the highest when we only use Intensity-based features. This shows that false positives were high in other cases when we add

structure-based features. It means that the classifier assume some of the non-nuclei pixels, probably around the boarder of nuclei, to be nucleus.

# 5 Conclusion

In this project, we were able to detect the nuclei in the skin biopsy images using AdaBoost with intensity-based and structure-based features. We ran the AdaBoost two separate times and then post-process the results with morphological functions. It turned out that using both intensity-based features and structure-based features and applying morphological functions on them gives the best recall while using only intensity-based features gives the best precision value. The results from nucleus labeling (finding the centroid of nucleus detected) is not perfect, as shown in Figure 6. If we have more time, we could iterate through the calculated centroids, find those with area that is too small and combine those with their closest centroids.

As a future work, we can try these tasks:

- Finding the boundary: for examining the shape and area of nuclei.
- Using nuclei to train a CNN for mitotic figures detection.

## References

Norman Casagrande. Automatic music classification using boosting algorithms and auditory features. 2006.

- Dan C Cireşan, Alessandro Giusti, Luca M Gambardella, and Jürgen Schmidhuber. Mitosis detection in breast cancer histology images with deep neural networks. In *International Conference on Medical Image Computing* and Computer-assisted Intervention, pages 411–418. Springer, 2013.
- Metin N Gurcan, Laura E Boucheron, Ali Can, Anant Madabhushi, Nasir M Rajpoot, and Bulent Yener. Histopathological image analysis: A review. *IEEE reviews in biomedical engineering*, 2:147–171, 2009.
- Adel Hafiane, Filiz Bunyak, and Kannappan Palaniappan. Fuzzy clustering and active contours for histopathology image segmentation and nuclei detection. In Advanced concepts for intelligent vision systems, pages 903–914. Springer, 2008.
- Jing Li and Nigel M Allinson. A comprehensive review of current local features for computer vision. *Neurocomputing*, 71(10):1771–1787, 2008.
- Cheng Lu and Mrinal Mandal. Automated segmentation and analysis of the epidermis area in skin histopathological images. In *Engineering in Medicine and Biology Society (EMBC), 2012 Annual International Conference* of the IEEE, pages 5355–5359. IEEE, 2012.
- C Ortiz de Solorzano, R Malladi, SA Lelievre, and SJ Lockett. Segmentation of nuclei and cells using membrane related protein markers. *journal of Microscopy*, 201(3):404–415, 2001.
- Sokol Petushi, Fernando U Garcia, Marian M Haber, Constantine Katsinis, and Aydin Tozeren. Large-scale computations on histology images reveal grade-differentiating parameters for breast cancer. *BMC medical imaging*, 6(1):14, 2006.
- Jelte Peter Vink and Gerard de Haan. No-reference metric design with machine learning for local video compression artifact level. *IEEE Journal of Selected Topics in Signal Processing*, 5(2):297–308, 2011.
- JP Vink, MB Van Leeuwen, CHM Van Deurzen, and G De Haan. Efficient nucleus detector in histopathology images. *Journal of microscopy*, 249(2):124–135, 2013.
- Carolina Wählby, I-M SINTORN, Fredrik Erlandsson, Gunilla Borgefors, and Ewert Bengtsson. Combining intensity, edge and shape information for 2d and 3d segmentation of cell nuclei in tissue sections. *Journal of microscopy*, 215(1):67–76, 2004.
- Ying Wang, Ping Han, Xiaoguang Lu, Renbiao Wu, and Jingxiong Huang. The performance comparison of adaboost and svm applied to sar atr. In *Radar*, 2006. *CIE'06. International Conference on*, pages 1–4. IEEE, 2006.